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First Named Inventor

DANNENMAIER, J.

Art Unit

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MENON, Krishnan S.

Attorney Docket Number

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Nov. 8, 2006

Reg. No.

31,716

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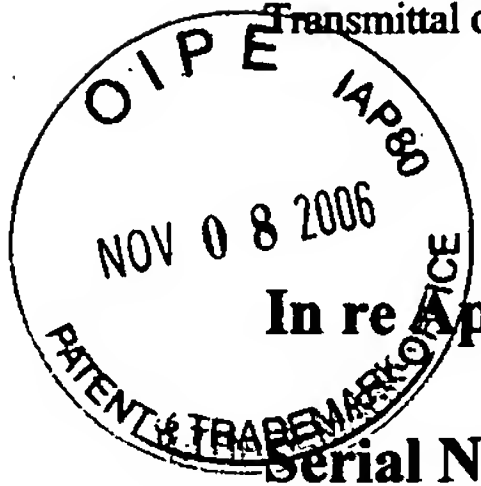
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**IN THE UNITED STATES PATENT AND TRADEMARK OFFICE**

**In re Application of: DANNENMAIER, Jürgen** )

Confirmation No. 2773

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**For: Filter Device Having More than One Filtration** )  
**Compartment** )

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Alexandria, VA 22313-1450

**TRANSMITTAL OF CERTIFIED COPY OF PRIORITY DOCUMENT**

Sir:

In response to the Office Action dated September 15, 2006, please find the certified copy of priority document EP Application No. 03008465.1.

It is believed that no fee is due for this submission. If this belief is in error, the Commissioner for Patents is authorized to charge the necessary fees to Deposit Account 03-2316.

If there are any questions, or if prosecution can be expedited in any manner by a telephone conference, the Examiner is urged to call Applicants representative at the below telephone number.

November 8, 2006  
Date

Respectfully submitted,

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**Patentanmeldung Nr.    Patent application No.    Demande de brevet n°**

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Der Präsident des Europäischen Patentamts;  
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Bezeichnung der Erfindung/Title of the invention/Titre de l'invention:  
(Falls die Bezeichnung der Erfindung nicht angegeben ist, siehe Beschreibung.  
If no title is shown please refer to the description.  
Si aucun titre n'est indiqué se référer à la description.)

Filter device having more than one filtration compartment

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11 April 2003

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Filter device having more than one filtration compartment

5 The present invention relates to a filter device for the filtration of fluids. In particular, one or more embodiments of the present invention relate to filter devices for use in dialysis-type treatments and for filtration processes similar to and related to the haemodialysis process, such as haemofiltration, haemodiafiltration and ultrafiltration, as  
10 well as to a method for making a housing of a filtration device.

Filter devices having hollow-fibre membranes are used inter alia (i.a.) in the area of dialysis for a wide variety of purposes. Such filters may thus also be referred to as dialysers, these being used for example in haemodialysis, in which blood is directed into  
15 and along the inside of the semi-permeable walls of the hollow fibres while dialysis fluid is directed around the outside of the hollow fibres. Various convection and diffusion processes may thereby take place across the walls of the hollow fibres. These processes serve for example to purify and to remove excess fluid from the blood. Additionally, the electrolyte concentration in the blood can be conditioned using infusion fluids, and  
20 buffers such as bicarbonate or acetate can be added to the blood. The haemodialysis process is effective at removing substances having a low molecular weight, but may be less effective at removing substances having a middle molecular weight. Low molecular weight substances in the context of dialysis typically include substances such as urea, having a molecular weight below 5kDa.

25 Filter devices of this type may also be employed in so-called haemofiltration, in which a substitution fluid is added to the blood. According to this process, the blood is directed through the inside of the hollow fibres, although in this case no dialysis fluid is passed around the outside of the fibres. Here, excess fluids, in particular water as well as waste  
30 products, are removed from the blood by means of a pressure difference across the membrane, here comprised by the semi-permeable walls of the hollow fibres. The

substitution fluid can be added either prior or subsequent to the filtration in pre- or post-dilution modes. Haemofiltration is more effective at removing substances having a so-called middle molecular weight lying within the range between approximately 5kDa-30kDa such as Beta-2-Microglobulin.

5

A further application for the present type of filter device includes haemodiafiltration: a combination of haemodialysis and haemofiltration, in which dialysate flows across one side of the membrane while blood flows across the other side and at the same time, a pressure gradient exists across the membrane. Infusion fluid may be added to the blood either prior to or after the filtration. This process can result in a higher filtration rate and is especially effective at removing substances having a low and middle molecular weight.

10  
15 A further process for which such filters may be used is known as plasmapheresis, in which aqueous blood-plasma is filtered out of the blood and returned to the blood after treatment.

Such filter devices are also used in filtration processes wherein undesirable substances may be removed from blood, water or other fluids.

20 The above-mentioned filter devices can equally be used as so-called ultrafilters for the production of substitution or infusion fluids. In this case, infusion fluid may be directed into the filter on one side of a semi-permeable membrane, and is filtered across the membrane by means of a pressure difference. In this way, the infusion fluid can be sterile-filtered by removal of endotoxins, bacteria and other contaminants. Ultrafilters  
25 generally have a similar construction to dialyser-type filters although they are generally smaller in dimension and are not generally used as dialysers in the dialysis process. Ultrafilters are usually employed during a blood filtration treatment in addition to a dialysis filter, the filtrate from the ultrafilter creating the infusion fluid which is then fed into the blood either on the blood side of the dialysis filter device or into blood in the  
30 blood tubes.

These filter devices are usually so constructed that the hollow-fibres are arranged as a loose bundle lying longitudinally within a tubular housing. The housing is provided at each end with an end-cap, and the hollow-fibre bundle is arranged between the ends of the housing so that the end-caps enclose the ends of the hollow-fibre bundle. The ends of the fibres are usually embedded within and secured by a potting compound made from a two-component polymer resin. Except as noted below, the potting compound completely surrounds the ends of the hollow fibres and is molded to the inside of the ends of the housing to create a seal between the header chamber and the inside of the tubular housing.

The extreme ends of the hollow fibres open out above the potting compound into a hollow space (hereafter: header-chamber) located in-between the end cap and the end of the hollow-fibre bundle. It is therefore possible, with the appropriate arrangement of inlets and outlets, to provide, in a manner known per se, various forms of filter such as the previously mentioned haemodialysis filters, haemofilters, haemodiafilters, ultrafilters etc.

Examples of the previously mentioned filters are disclosed in EP-0 305 687, EP-0 355 325 and EP-0 525 317.

The previously mentioned filters or dialysers have certain features in common, namely, that a first fluid may be directed into and through the inside of the semi-permeable hollow fibres. This first fluid may exit from the fibre column having had certain substances removed and possibly certain substances added. A second fluid may be present on the outside of the hollow fibres. This second fluid can either flow through the housing, past and around the hollow fibres, via appropriately located inlet and outlet means; or it can be removed from the first fluid and directed out of the housing via a suitable outlet, for example by means of a pressure differential across the hollow-fibre membrane. This second fluid may be a purified form of the first fluid, a dialysis fluid for the exchange of substances into and out of the first fluid across the hollow-fibre membranes, or a waste fluid removed from the first fluid, inter alia.

If one of the aforementioned filters is applied in the area of dialysis, for example in haemodialysis, various fluid lines (conduits) are connected to it. These fluid lines on the one hand lead blood from the patient to the blood side of the filter and then back to the patient. Additional fluid lines lead the dialysis fluid from a dialysis fluid supply, controlled by a dialysis machine also sometimes referred to as a dialysis monitoring device, to the dialysate side of the filter and after passage through the filter further to a drain. The blood side here refers to the area of the filter through which the blood of the patient is led, while the dialysate side refers to the area of the filter or the filter housing through which the dialysis fluid is lead. The blood side and the dialysate side are separated from each other in the filter housing by one or more semi-permeable membranes and these sides correspond respectively to the sides along which the previously mentioned first and second fluids pass.

In order to improve the effectiveness of blood filtration treatments, it is known to use more than one filtration process or filter device connected in series. As an example, a haemofiltration process may be combined in series with a haemodialysis or haemodiafiltration process, thereby necessitating more than one filter device.

It has further been proposed to combine more than one filtration device within a single housing. A filter cartridge comprising more than one filtration compartment is disclosed for example in WO 02/47785. According to the device disclosed in this document, two hollow-fibre bundles are arranged in adjacent compartments which are separated by a wall in which a communicating aperture is provided for the flow of filtrate or dialysate through both compartments.

Additional considerations with regard to the use of such filtration devices are also relevant for their design. When setting up known filter devices prior to a filtration treatment, a number of set-up operations are required to be performed by trained personnel. In particular, extracorporeal blood tubes as well as any necessary dialysis fluid tubes must be connected to the appropriate fluid flow ports of the filter device. In

- addition, a separate ultrafilter is often desired to be connected to an infusion fluid supply. This must be carried out with care, as the tubes must be connected correctly in order to avoid potential dangers arising from an incorrect set-up. The set-up stage can be time-consuming and therefore reduces the number of treatments which can be carried out using a particular monitoring device. In addition, the requirement to use a separate filter device for ultrafiltration, as well as possibly more than one filter device for filtering blood, increases the equipment costs for each treatment and also the number of connections required.
- 10 A further dialyser device is known from DE-A-196 07 162, in which a filtration device for substitution fluid is disclosed along with a haemodiafiltration device integrated within a single housing. Filter membrane means in the form of hollow fibres are provided within both compartments. One end of the hollow fibres of the filter for a substitution fluid is sealed off by means of potting compound or by a cover. A problem encountered
- 15 with this device is that it is difficult to completely expel all of the air contained within the compartment for the substitution fluid at the start of a filtration process, both the air around the outside of the hollow fibres and in the inside of the fibres. Air on the inside of the fibres is pushed by liquid passing across the membranes into a header chamber at either the blood entry or exit of the dialysis compartment thereby causing unnecessary
- 20 contact between blood and air in the blood flow circuit. This may be avoided by passing substitution fluid through the filtration compartment prior to passing blood through the haemodiafiltration compartment although this involves additional work for an operator. In addition, air around the outside of the membranes is not completely expelled during the initiation phase of filtration and may be fed through into the blood during a treatment.
- 25 This increases the thrombogenicity of the blood filtration process. A further drawback of this disclosure exists in that filtration of the substitution fluid takes place from the outside through to the inside of the hollow-fibre membranes. This necessitates using a different kind of hollow-fibre than those used for the filtration of blood in the haemodiafiltration process in the neighbouring chamber, because the direction of the pore size gradient across the membrane thickness requires to be inversed. This requirement
- 30 greatly complicates the manufacturing requirement of such a device. In addition, when

manufacturing a device according to this disclosure, the filling of the respective compartments with hollow fibres is rendered complex and costly.

5 In order to overcome some of the problems associated with known filter devices, a filter device is provided according to the present invention, in which at least two fluid filtration compartments are provided within a filter housing, the respective compartments being separated by a continuous internal wall. In this way, more than one fluid may be filtered at any one time by filter means in respective separate chambers of a single filter device. A first surface of the filter membrane means is in communication with both an inlet and  
10 an outlet. A device according to the invention is defined in claim 1. Preferred features of the invention are defined in the dependent claims.

According to the invention, filter membrane means in each compartment each have a first and a second surface, wherein the first or second surface are each in fluid communication  
15 with respective external flow ports. The external fluid flow port may be connected to a fluid supply or drain means, which fluid supply or drain means are located externally of the filter housing. Alternatively, an external fluid flow port may be connected to an inflow port in fluid flow communication with a separate filtration compartment to thereby lead away fluid emerging from a second surface of filter membrane means to be infused  
20 in a fluid involved in a separate filtration treatment in another filtration compartment. For example, an infusion fluid having passed across a filtration membrane may be channelled to an inflow or outflow section of an adjacent filtration compartment in which blood is filtered.

25 A first surface of the filter membrane means in each compartment is in communication with an inlet and an outlet of a fluid filtration compartment thereby ensuring that air may be effectively expelled from each compartment during an initial phase of operation of each filter. The filter device of the invention may be operated in such a manner that fluids to be passed across a membrane means in any compartment may be passed from a  
30 first surface to a second surface of the membrane means. Where the membrane means are hollow fibre membranes, ultrafiltration usually takes place by passing fluid at a higher

pressure through the inside surfaces of the fibre membranes. The fluid then passes through to the outside surface and is filtered in the process. Alternatively, fluid may also be passed from second, exterior surfaces through to the first, inside surfaces of hollow fibre type membranes. Filtration may be carried out from the outside surface to the inside surface using a conventional type of fibre or alternatively, using a special fibre, the walls of which are adapted for filtration in the said direction. Such fibres may be made from a more rigid material than conventional fibres.

The filter membrane may be comprised of a bundle of hollow-fibres, preferably semi-permeable membrane fibres, in which case the first surface designates collectively the insides of the hollow fibres in the bundle and the second surface designates the outside surfaces of the hollow fibres.

Where hollow-fibres are employed as filter membrane means, the outside surfaces of the hollow-fibres are in communication with the external fluid flow port in the above example. The aforementioned continuous internal wall (or walls) within the filter device of the invention divide the interior of the filter housing into separate filtration compartments, such that there is no fluid communication across the wall (or walls) between the respective filtration compartments.

The filter device of the invention may be configured such that the respective first surface (or first surfaces) of the filter membrane means in one compartment are in fluid flow communication with the respective first surface (or first surfaces) of filter membrane means in at least one other compartment. This enables a fluid to be passed through more than one filtration process in series. Such a configuration enables, for example, different filtration conditions to exist in respective filtration compartments. Alternatively, or additionally, the second surface (or surfaces) of a filter membrane means in a filtration compartment may be in fluid flow communication with a first surface (or surfaces) of a filter membrane in another compartment. In this way, for example, the fluid having been purified by passing across the filter membrane of one compartment may be added to the fluid being or having been filtered in another compartment. This may be achieved, for

example by means of an external flow port from one filtration compartment being connected for channelling fluid to an inlet or outlet for fluid entering or leaving a first surface of a filter membrane in another compartment.

- 5 The housing means of the filter device of the invention may generally have elongate longitudinally extending walls which may be of any appropriate cross-section, e.g. tubular, circular, elliptical, rectangular, or any other suitable geometry. The longitudinal walls include at least one external wall continuous or discontinuous about the circumference, and one or more internal walls extending between opposite ends of the  
10 housing. The one or more internal walls divide the interior of the external housing into two or more internal compartments.

- The possibility of carrying out a blood filtration treatment at the same time as an ultrafiltration process is especially advantageous. According to a preferred feature of the  
15 invention, more than one blood filtration process may be carried out in addition to an ultrafiltration. For example, the outlet portion of the hollow-fibres in one filtration compartment may be in fluid communication with the inlet portion of a bundle of hollow fibres in another compartment of the filter device. A replacement infusion fluid ultrafiltered in one compartment of the filter device may then be added to the blood at  
20 any stage in the blood filtration process before, after or in one or more of the other compartments of the filter device; e.g. before passage of the blood through the membranes (pre-dilution), between successive treatments (mid-dilution) or after one or two (or more) treatments (post-dilution).

- 25 According to preferred features of the invention, there may be provided two or three or more separate filtration compartments for carrying out simultaneous and/or successive filtration treatments. Where three or more compartments are provided, a first fluid such as an infusion fluid may be treated in a first compartment while a second fluid (usually blood; the first fluid being an infusion solution described above) may be subjected to  
30 more than one filtration process in series. For example, a haemofiltration treatment may be carried out in a second compartment, the fluid thereby removed from the second fluid

escaping from the filter through an external fluid flow port. The second fluid emerging at a fluid outlet of the membranes of the said second compartment may then be directed into the filtration membranes of a third filtration chamber.

- 5 Where semi-permeable hollow fibres are used as a filter membrane means, these may be held in place at their ends by a so-called potting compound. The potting compound may consist of a hardened polymer resin, such as two-component polyurethane, molded to the internal walls of the tubular housing and serves as a barrier enclosing the second surface of the membranes within a compartment of the tubular housing. It also maintains the  
10 apertures of the hollow fibres such that the (internal) first surfaces of the fibres are open at an outlet or inlet end of the housing. The ends of the housing are advantageously enclosed by end-caps, thereby providing so-called header chambers.

- Each end-cap may be constructed so as to enclose more than one header chamber, with  
15 each header chamber being provided with at least one fluid inflow or outflow port, and possibly with one or more additional fluid flow ports, for example for supplying additives to the fluid within the header chamber. In particular, each end-cap may enclose each header chamber in correspondence with each of the filtration compartments internal of the overall filter housing. The header chambers of a single end-cap may be separated  
20 from one another by wall means and by a seal member placed between the header chamber wall and an internal wall and/or the surface of the potting compound in order to prevent migration of fluid from one header chamber to another. Alternatively, the hollow fibre bundle of more than one filtration compartment may open out into a single header chamber. This may be useful for a filter device intended for mid-or post-filtration  
25 dilution with a filtered infusion solution or to provide serial filtration of a fluid in more than one filtration compartment. Alternatively, separate header chambers may be connected for fluid flow by connecting together fluid flow ports of respective header chambers using molded or tubing line conduit means.

- 30 The housing of the filter device may be provided, as already mentioned, with any appropriate cross-section. The housing comprises continuous internal walls which divide

the filter into separate filtration compartments. No single compartment would thereby be delimited entirely by peripheral or external walls of the housing, each compartment being delimited at least partly by an internal wall. The housing may for example be tubular, and in one embodiment may be made up of two separate longitudinally extending sections of a housing wall. The respective portions of the housing may be joined together along seam-type joints by any suitable means such as by bonding or welding e.g. using ultrasound or laser welding. In the case of laser-welding techniques, the two sections of the filter housing would benefit from particular light reflective properties in order to ensure an adequate weld. For example, one of the housing sections may be made from substantially clear, uncoloured material, while the other may contain a light-reflective dye suitable for causing plastics material at the boundary of the two housing portions to melt sufficiently to form a bond. In a possible embodiment of a laser-welded housing, one housing portion may be made from polycarbonate while another section may be made from polypropylene.

Assembly of the filter device may be achieved by combining the steps of filling the respective filtration compartments as initially defined by the separate sections with hollow-fibres and then assembling the housing. For example, hollow-fibres may be placed within the respective filtration compartments defined by each respective single section of the housing. The housing sections may then be brought together and fixed in position enclosing the respective fibre bundles in their compartments. The housing which is here, by way of example, shown tubular sections may thereby each include corresponding portions of internal walls, whereby the respective edges of the various corresponding wall portions would then desirably be bonded to one another as would the outer walls of the said sections. Bonding may be carried out by any suitable method such as by using adhesive means or by welding as described more fully herein.

Alternatively, the internal wall may not be in portions but instead may be provided integral with a first one of the tubular housing sections, with the second section comprising only an outer wall portion of the housing joined on its internal face to the respective internal and outer wall portions of the aforementioned first section. In either

the previous or this latter case, the first section is likely to be somewhat larger than the second section. For example, the first section may make up more than half of the outer circumference or periphery of the resulting housing, while the second portion may make up less than one half of the outer periphery, perhaps as little as one third or one quarter.

5 In the case of say a generally rectangular tubular housing of the filter device, one side of the cross-sectional rectangle may be comprised of the said second portion or cover portion, while the main first portion of the housing could comprise substantially three sides of the said cross-sectional rectangle. In this case, internal walls could advantageously be provided integral with the said first portion, or with both portions.

10

In order to improve in one embodiment the methodology for assembling a multi-compartment filtration device, at least one outer wall of a respective filtration compartment may be provided parallel to an internal wall of a same compartment. This feature may enable a more optimal filling of the fibre bundle within each compartment.

15

An end of the housing portion may be provided with one or more apertures or recesses for engaging the potting compound which restrains the ends of the hollow fibre bundles. In addition, there may be one or more apertures provided adjacent the ends of the tubular housing which provide for inflow or outflow of liquid into or from an internal  
20 compartment of the housing around the second surfaces (the outside) of the hollow-fibres. Such an embodiment may be useful when the end-caps are provided with fluid flow ports for more than one fluid intended to be channelled towards different surfaces of the hollow fibres. In such a case, the fluid intended to flow around the outside of the hollow fibres may flow through a peripheral flow port of an end-cap and around a channel formed and  
25 bounded by a sill portion of the tubular housing and then through a filtration compartment of the tubular housing.

The present invention also encompasses a method of making a filter housing of the invention in which the housing is made from two longitudinally extending portions which  
30 are bonded together along seam-type joins. A preferred method of bonding is by welding, in particular by laser or ultrasound welding.

The following drawings are included by way of example of some embodiments of the invention.

- 5 Fig. 1: An external isometric view of a filter device with two chambers;  
Fig. 2: A longitudinal section view of the device shown in Fig. 1;  
Fig. 2a: A longitudinal section view of an alternative construction of the filter device such as shown in Fig. 2.  
Fig. 3: A partial longitudinal section view showing detail of an end of a filter device  
10 shown in Figs 1 and 2;  
Fig. 4: A cross-section view of a middle portion of a filter device as shown in Figs 1-3;  
Fig. 5: A cross-section view of an end portion of a filter device as shown in Figs 1-3;  
Fig. 5a: A cross-section view of an end portion of an alternative construction of the filter device shown in Fig. 5.  
15 Fig. 6: A detailed view of one end of a housing with the header cap removed.  
Fig. 7: An isometric view of a filter device having three filtration compartments  
Fig. 8: An isometric partial view of an end of the housing of the filter device of Fig. 7  
Fig. 9 and 9a: A longitudinal section view of a three compartment filtration device  
Fig. 10: A cross-section of an end of the filtration device of Fig. 9.  
20 Fig. 11 and 11a: End views of a dismantled and assembled shell portion of a housing  
Fig. 12: An isometric view of a disassembled housing  
Fig. 13 and 13a: End views of a further dismantled and assembled housing

25 The filter device shown in Figures 1, 2 and 3 comprises a housing 1 and two end-caps 13 and 14, one arranged at each end of the housing. The housing 1 is comprised of a longitudinally extending generally tubular wall having two opposed ends. Respective compartments 2 and 3 are separated by a continuous wall means 8. Filter membrane means (not shown) are arranged longitudinally within respective filtration compartments 2 and 3 (Fig. 2 and 3). These usually each comprise a bundle of semi-permeable hollow  
30 fibres secured at their ends by a potting compound 12 (Fig. 3) which extends around an end portion of the wall of the housing 1. The open ends of the hollow fibres, embedded

in the potting compound 12 constitute inlet or outlet apertures 4a, 4b and 5a, 5b for fluid entering or leaving a filtration compartment along a first surface of the filter membrane means therein. In the case illustrated, the open apertures 4a, 4b and 5a, 5b of the ends of the hollow fibres open out into a respective header chamber 17, 18 arranged within the  
5 end caps 13, 14.

Fluid inflow and outflow ports 6, 7, 15, 15a, 16 and 16a for respective first and second fluids are arranged on the end-cap 13 and 14. Ports 15 and 16 and 15a and 16a are in fluid flow communication with header chambers 17, 18 and 17a, 18a inside each end-cap  
10 13, 14 and with a first surface of the filter membranes of each filtration compartment 2, 3. External fluid flow ports 6, 7 and 11 are illustrated provided in fluid flow communication with a respective second side of the filter membranes of the respective filtration compartments 2, 3 arranged within the housing 1. The fluid flow ports 6, 7, 11 could optionally be provided on portions of the wall of the housing 1 nearby but not necessarily  
15 integral with an end-cap as shown in Figs. 2 and 2a.

A conduit means 19 may be provided for conducting a fluid emerging from the second surface of the filter membrane of a filtration compartment 3 via an external fluid flow port 7 and an optional additional fluid inflow port 22 (see Figs 1 and 3) into the header  
20 chamber 17 which is in fluid flow connection with another fluid passing along a first surface of filter membrane means of the separate filtration compartment 2. In this way, for example, the ultrafiltrate emerging from an ultrafilter arranged in filtration compartment 3 within the housing 1 may be used to dilute another fluid such as blood, being filtered, by haemofiltration or haemodialysis or haemodiafiltration in additional,  
25 discrete filtration compartment 2. Under normal circumstances, the infusion fluid is generated in a filtration compartment at a higher pressure than the pressure of the first fluid such as blood in the inflow or outflow area of the filtration compartment into which the infusion fluid is subsequently directed. As a precautionary measure, a check or non-return valve (not shown) may be present in the conduit means 19 in order to prevent  
30 accidental passage of blood from a blood filtration compartment into an ultrafiltration compartment.

As can be seen, the potting compound 12 can be anchored to the housing 1 at a peripheral region and can enclose a lip or flange portion 23 formed at the end of the housing 1. The potting compound 12 may additionally be anchored to the housing at apertures 20, 20a in the housing. The apertures 20, 20a are provided in two rows in the example illustrated at Fig. 3, and serve to allow the flow of fluid between the enclosed peripheral channels 24, 24a and respective internal filtration compartments 2 or 3 to the second surface (or the exterior surface) of the hollow fibres. The apertures 20, 20a comprise two sets of holes communicating with two separate channels 24, 24a (see Fig. 3). One set of holes 20 communicates with chamber 2 while the other set 20a communicates with chamber 3. These apertures 20, 20a may additionally serve as anchoring means for the potting compound 12 which may flow through some of the apertures while in a liquid phase prior to hardening. To this end, a sill or flange 27 may be provided integral with the housing 1 such that when an end-cap 13, 14 is disposed in place upon the housing 1, the channels 24, 24a are present in the space created by the header cap peripheral wall and the housing 1. Inlet ports 6 and 7 can therefore be provided in a lateral or peripheral portion of the end-cap 13 for inflow or outflow of fluids to or from the outside of the hollow fibres.

In the device illustrated in Figure 2, infusion fluid to be purified may be fed into the filtration compartment 3 through inflow port 25. The fluid then passes into a lower header chamber 18a of the end-cap 14 which communicates with filtration compartment 3, after which it passes along the inside surface (first surface) of the hollow fibre membranes of the fibre bundle inside the filtration compartment 3. In order for the fluid to penetrate inside the fibres during an initial priming stage, the outlet flow port 16 is held open for air to escape from the filtration compartment 3 before it becomes filled with infusion fluid. The outlet port 16 may then be closed when infusion fluid has filled the filter membranes, after which the infusion fluid is forced by a pressure gradient across the membranes through to the second, exterior surface of the membranes, from where it leaves the filtration compartment 3 through external flow port 7.

The two header chambers 17, 18 are clearly visible in Fig. 3, separated from one another by wall portion 28 of the end-cap 13 and by an additional seal 21. A conduit 19 is partly shown, this being provided connected to flow port 22 and also to the outlet port 7 for the first fluid e.g. ultrafiltrate, emerging from the first filtration compartment 3. This corresponds to either a pre- or post-dilution set-up, in which infusion fluid entering the header chamber 17 via fluid flow port 22 is infused into a second fluid prior to or after passing through the hollow fibre bundle contained within the filtration compartment 2. The second fluid could be made to flow in either direction (up or down) in this example.

A possible construction of the filter device, in particular, the housing of the filter device can be appreciated from Figures 4 and 5. Two sections 41 and 42 of the housing 1 are shown joined at seams 35 of peripheral wall portions 51, 50 as well as at internal wall portions 48, 49 which together make up continuous internal wall 8 and which furthermore define internal surfaces 52 and 53. As introduced above, end-cap 14 may comprise a fluid inflow port 11 which may be molded integrally therewith and which may allow fluid such as for example dialysis fluid to flow to or from the outside surface or surfaces of membrane means within compartment 2. During the fabrication of the device, fibre bundles may be laid within the compartments 2 and 3 prior to closing the compartments by joining section 42 to section 41. In order to increase the density of the fibres within the housing, the wall surfaces 50, 51, 52 and 53 are arranged to be substantially parallel. The internal wall portions 48, 49 may advantageously be provided hollow along one or more portions of their length, in order to reduce material usage and for uniformity of wall thicknesses throughout the housing portions. In Fig. 5, the enclosed channels 24, 24a are shown allowing fluid to flow to or from port 11 and into or out of a filtration chamber 2 via apertures 20, 20a. Similar channels 24, 24a (not shown in Fig. 4 or 5) are provided in the upper end cap 13. The apertures 20 in filtration compartment 2 are kept separate from the channel 24a and apertures 20a of filtration compartment 3 by means of either a seal (not shown) or by additionally including barrier means (not shown) between the internal wall portions 48, 49 and the outer regions of the wall of end cap 14.

In Fig. 6, the end portion of a housing according to an embodiment of the invention is illustrated. As introduced in Figs 2 and 3 above, a sill 27 around an outside portion of the wall of the housing 1 is shown, around which an end cap may be sealingly fitted. An upper portion of the housing wall is provided with apertures 20 which serve two purposes. On the one hand, these apertures serve to provide an anchoring means for the potting compound 12 which secures the hollow fibres. In addition, some of the apertures serve as inlets into the filtration compartment on the outside surface of hollow fibres contained therein. The fluid may thereby be distributed into the compartment inflowing from the external port. Seal means 21 (as shown e.g. in Fig. 3) are shown in position corresponding to the positions of the respective housing outer walls and the inner walls separating the respective filtration compartments 2 and 3.

In Figs 2a and 5a, there is shown a possible embodiment of the filter device in which only the filtration compartment 2 intended for dialysate fluid flow in a blood filtration process is provided with liquid distribution apertures 20 at the ends of the compartment. Dialysis liquid may thereby flow first through fluid flow port 6 and to the outside of the filter membranes inside filtration chamber 2 via the peripheral channel 24 and the distribution apertures 20. In this embodiment the ultrafiltration compartment 3 is provided with an external flow port 7a on the wall of the housing 1. The arrangement shown in Figs 2a and 5a avoids the potential need for an additional seal or wall component possibly requiring welding between the internal walls separating the respective chambers 17 and 18 and the inside of the end-cap 13 of the previously described embodiment.

In Figs. 7-10 with first reference to Figs. 7 and 8, a filter device having three internal filtration compartments within a unitary housing 101 is illustrated. In this case, a first filter e.g. an ultrafiltration filter is provided in a compartment 103 located adjacent and in between two outer dialysis-type filtration compartments 102, 104. Fluid flow ports 106 and 107 allow fluid such as dialysis fluid to enter or leave filtration compartments communicating with a second surface of filter membranes provided therein. In the example shown, these are provided at a peripheral portion of an end-cap 113, although they could also be provided on the wall of the housing 101 (see the example of Figs. 2a

and 5a). Distribution apertures 120 may be used to ensure anchoring of the potting compound (not shown) and allow inflow and outflow of fluids via an enclosed channel 124 as in the two-compartment model described previously. In the embodiment shown, fluid inflow and outflow means to the second surface of the filter membranes of the ultrafiltration compartment 103 may be provided molded integrally with the wall of the housing 101. A conduit 119 may provide for infusion fluid emerging from compartment 103 via port 109 to flow into a header chamber within end-cap 113 via inlet port 122, where it is added to another fluid, e.g. blood filtered via the first surfaces of filtration membranes in either or both of compartments 102 and 104.

In Figs 9, 9a and 10 a three compartment device is shown in respective longitudinal section and in cross section. The internal compartments of the device are defined by two wall portions 148 and 149 joined at seam portions 35. These define between them a central compartment 103, and two outer compartments 102 and 104. Some internal walls of the device are in parallel configuration in order to optimize the filling of the internal spaces with hollow fibre membranes. From Fig. 9, 9a it can be seen from arrow A that header chamber 117 within the upper end-cap 113 may be configured such that the respective first surfaces of filter membrane means within compartments 102 and 104 can be disposed in fluid flow communication. This enables, for example two different blood filtration type processes to be carried out simultaneously and/or in series within a single filter device, in addition to an ultrafiltration step of e.g. an infusion fluid. The infusion fluid in the arrangement may be added to the blood via exit flow port 109 (Figs. 7 and 8), through conduit 119 (Figs. 7 and 8) and an additional inflow port 122 (Fig. 7) in the header chamber 117 in an arrangement corresponding to a mid-dilution step. Flow port 115 is optional and may serve for fluid inflow or outflow or may serve to bleed air from the compartment 104 while it is being filled with e.g. blood or otherwise being primed, before being sealed again prior to the commencement of filtration.

The wall members 130 and 131 (Fig. 10) may keep separate the dialysate flowing around channel 124 into or out of chambers 102 and 104. The wall means could be replaced by an equivalent seal means (not shown).

In use, an infusion fluid may be passed into the flow port 125 (Fig. 9) as indicated by arrow B. During initial filling of the compartment 103 (e.g. during priming), air may be let out through flow port 116. Once the compartment 103 is filled, the flow port 116  
5 may be sealed and purified infusion fluid (or other priming fluid which may be used) flows across the membrane means of the filtration compartment 103 emerging from a second surface of the membrane means through a fluid outlet 109 as shown in Fig. 7. The fluid may be channelled into the header chamber 117 via conduit 119 already described. A second fluid, usually blood, may be passed through the filter device in the  
10 direction of arrow C first through flow port 128 into filtration compartment 104 along a first surface of filter membrane means therein (not shown). Air may be bled from the chamber at port 115 (e.g. during priming or during use), before the blood flows across the header chamber 117 along the direction of arrow A and onto the first side of filter membrane means in compartment 102 before exiting along the direction of arrow D at  
15 flow port 126. As an alternative to providing a communicating header chamber between respective filtration compartments, a conduit could be connected to fluid flow ports of whichever header chambers it may be desired to connect. Dialysis fluid may be passed into the compartments 104 and 102 via flow ports 107 and 111 respectively and may exit the compartments through ports 106 and 110. Alternatively, as in haemofiltration, fluid  
20 may be removed without addition of dialysis fluid, in which case corresponding inflow ports may be kept sealed. As is obvious, the device shown in Fig. 9 may be operated in a number of combinations of filtration processes described previously in this specification.

In Figs. 11, 11a, 12, 13 and 13a, various possibilities are shown for connecting together  
25 shell portions 41, 42, 141, 142 of housing 1, 101. Figs 11, 11a and 12 show a possibility in which a two-compartment housing 1 is formed from hinged housing shell sections 41, 42. Continuous wall means 8 consists of wall portions 48 and 49. As an alternative (not shown) the wall means 8 could be made from a single wall portion either integral with one shell portion 41 or 42 or it could be fixed to the shell portions 41, 42 using a bonding  
30 technique. Numeral 160 denotes fluid flow ports in general which may be inflow or outflow ports. In the Figures 11, 11a, 12, 13 and 13a the flow ports 160 are shown

schematically integral with walls of housing 1, 101, although these could equally well be provided at end-caps of the filter device. The hinged housing 1 could be employed for a three-compartment type device or for a device with more than three compartments. Bonding of the housing 1 is achieved by welding or by adhesive means along seam 35, 135 (see also Fig. 4). Figs. 13 and 13a show a similar housing 101 in two parts which are shell portions 141 and 142. These are bonded or welded along laterally and longitudinally arranged seams 135. The device of Figs 13 and 13a is shown with three compartments 102, 103 and 104, although the same technique could be employed for a device having only two compartments or for a device having more than three compartments. As in Figs. 11, 11a and 12, the continuous wall portions 8 could be provided either from wall portions 148 and 149 or from a single portion attached to only one shell segment or added as a separate element. Furthermore, the respective portions may be held in an opened position as shown in Figure 12 for filling with filter means such as hollow fibre bundles in each respective compartment of shell portion 41 or 141 before completing the housing 1, 101 by closing shell portion 42, 142 on top of said portion 41 in which filter means are laid longitudinally.

In all of the embodiments illustrated and described above, the internal wall portions 48, 49, 148, 148 may be welded together or bonded to thereby create internal walls 8 and to generate an integral filter housing. One method of welding includes laser welding as mentioned or welding using other electromagnetic means. The welding may be carried out while filter means such as membranes in the form of hollow fibers are in place within respective chambers in the housing. Materials used for the housing may advantageously include materials having particular light reflective properties in order to ensure an adequate weld. For example, one of the housing sections may be made from substantially clear, uncoloured material, while the other may contain a light-reflective dye suitable for causing plastics material at the boundary of the two housing portions to melt sufficiently to form a bond. In another possible embodiment of a laser-welded housing, one housing portion may be made from polycarbonate while another section may be made from polypropylene. The different refractive indices of the materials may produce sufficient

heat for a weld to form when laser or electromagnetic radiation is aimed at the join or seam 35, 135.

## CLAIMS

1. Filter device comprising a housing (1, 101), said housing (1, 101) enclosing at least two fluid filtration compartments (2, 3, 102, 103, 104), wherein each filtration  
5 compartment (2, 3, 102, 103, 104) comprises respective filter membrane means having a respective first and second surface, said first surface of each filter membrane means being in fluid communication with an inlet of each said filtration compartment (2, 3, 102, 103, 104), said second surface being in fluid communication with at least one external fluid flow port (6, 7, 7a, 11, 106, 107, 109, 110, 111) of each said filtration compartment (2, 3,  
10 102, 103, 104), and wherein respective adjacent filtration compartments (2, 3, 102, 103, 104) are separated from each other by continuous internal wall means (8) such that more than one fluid may be filtered simultaneously by said filter device.
2. Filter device according to claim 1, comprising two filtration compartments (2, 3)  
15 arranged within said housing (1) and wherein one of said filtration compartments (3) is suitable for carrying out ultrafiltration of a first fluid while the other compartment (2) is suitable for simultaneously carrying out either haemofiltration or haemodialysis or haemodiafiltration of a second fluid.
- 20 3. Filter device according to claim 1, wherein said device comprises a housing (1, 101) within which are arranged at least three filtration compartments (102, 103, 104) and wherein at least one of said filtration compartments (103) is suitable for carrying out ultrafiltration of a first fluid while each of the other compartments (102, 104) is suitable for simultaneously carrying out either haemofiltration or haemodialysis or  
25 haemodiafiltration of a second fluid.
4. Filter device according to claim 3, wherein said first surfaces of at least two of said filter membrane means in separate filtration compartments (2, 102, 104) are in fluid flow communication.

30

5. Filter device according to any preceding claim, wherein said second surfaces of said filter membrane means of one said filtration compartment (3, 103) are in fluid communication with said first surface of said filter membrane means in another of said filtration compartments (2, 102, 104).

6. Filter device according to any preceding claim, wherein said first surface of said filter membrane means of one said filtration compartment (3, 103) is in fluid communication with said second surfaces of said filter membrane means in another of said filtration compartments (2, 102, 104) via said external fluid flow port (7, 7a, 109).

7. Filter device according to any preceding claim, wherein said filter membrane means comprises a bundle of semi-permeable hollow-fibre membranes and wherein said first surface is comprised of the interior surfaces of said hollow-fibres in said bundle and wherein said second surface is comprised of the exterior surfaces of said hollow-fibres in said bundle.

8. Filter device according to claim 7, wherein said housing (1) comprises two opposed ends and a tubular external wall therebetween, said hollow-fibre membranes being arranged within each of said filtration compartments (2, 3, 102, 103, 104) along the longitudinal direction of said tubular housing (1), wherein the ends of said hollow fibre membranes are secured by and embedded within a potting compound (12).

9. Filter device according to claim 8, wherein an end-cap (13, 14, 13, 114) is fixed to each end of the tubular housing (1) and wherein a header chamber (17, 18, 117, 118) is provided between each said end-cap (13, 14, 13, 114) and the ends of said hollow fibres.

10. Filter device according to claim 8 or 9, wherein said external wall of said tubular housing (1) is provided at its ends with engagement portions (20) for positively engaging said potting compound (12).

11. Filter device according to claim 10 wherein said engagement portions include one or more apertures (20) at each end of said external wall.

12. Filter according to any of claims 9-11, wherein each said header chamber (17, 18, 117, 118) is divided into separate chambers in respect of each filtration compartment (2, 3, 102, 103, 104), each separate header-chamber (17, 18, 117, 118) being provided with a fluid flow port (15, 16, 25, 26, 115, 116, 125, 126, 128).

13. Filter according to claim 12, wherein respective header chambers (17, 18, 117, 118) within a single end-cap (13, 14, 113, 114) are separated from one another by means of a wall portion (28) and a sealing member (21).

14. Filter device according to claim 12 or 13, wherein respective separate header chambers (17, 18, 117, 118) are in fluid flow connection, such that a first fluid emerging from a first filtration compartment (3, 103) may be directed from one header chamber to another header chamber from which the first fluid passes into filter membrane means of a second filtration compartment (2, 102, 104).

15. Filter device according to any preceding claim, wherein conduit means (19, 119) are provided for channeling fluid emerging as a filtrate from said second surfaces of one of said filter membrane means in a first compartment (3, 103) through an external fluid flow port (7, 7a, 109), into a fluid flow port (22, 122) in fluid communication with another fluid passing across said second surfaces of filter membrane means in another one of said filtration compartments (2, 102, 104).

16. Filter device according to any preceding claim, wherein said tubular housing (1) is comprised of two longitudinally extending shell portions (41, 42) joined together along one or more longitudinal seams (35).

17. Filter device according to claim 16, wherein the two said longitudinally extending shell portions (41, 42) are welded together.

18. Filter device according to claim 17, wherein said two said longitudinally extending shell (41, 42) portions are laser welded.
- 5 19. Filter device according to claim 17, wherein the two said longitudinally extending shell portions (41, 42) are ultrasound welded.
20. Filter device according to any of claims 16-19, wherein one of said longitudinally extending shell portions (41, 42) of the tubular housing (1) describes less than one half of  
10 the circumference of the wall of said tubular housing (1).
21. Filter device according to any of claims 16-20, wherein at least two internal facing walls (50, 51, 52, 53) of respective filtration compartments (2, 3, 102, 103, 104) are in a parallel relationship to each other.  
15
22. Filter device according to any of claims 16-21, wherein respective said longitudinally extending shell portions (41, 42) of the tubular housing (1) are made from mutually different materials selected from the group including polymeric materials.
- 20 23. Filter device according to any of claims 1-22, wherein said first surface of each said filter membrane means is in fluid communication with an inlet and an outlet (4a, 5a, 4b, 5b) of each said filtration compartment (2, 3, 102, 103, 104).
24. Filter device according to any preceding claim, comprising at least three discrete  
25 filtration compartments (2, 3, 102, 103, 104), wherein two of said compartments (2, 3, 102, 103, 104) are suitable for carrying out serial dialysis or haemodiafiltration or haemofiltration or any combination of said processes.
25. Use of a filter device according to any of claims 1-24, for simultaneously carrying  
30 out ultrafiltration of a blood infusion fluid and one filtration treatment of an additional

fluid, said filtration treatment selected from either haemofiltration, haemodiafiltration or haemodialysis.

26. Use of a filter device according to claim 3 and any of claims 4-24, for  
5 simultaneously carrying out ultrafiltration of a blood infusion fluid and at least two filtration treatments of an additional fluid, said filtration treatments selected from either haemofiltration, haemodiafiltration or haemodialysis.

27. Use of a filter device according to claim 25 or 26, wherein an infusion fluid  
10 emerging from said ultrafiltration is channeled into the said second fluid.

28. Method of making a filter device according to any claim 1-24, wherein the housing (1) is comprised of two longitudinally extending shell portions (41, 141, 42, 142) which constitute external walls of the housing (1, 101) and internal walls (50, 51, 52, 53) separating respective filtration compartments (2, 3, 102, 103, 104) within the housing (1, 101), the method comprising bonding together the said shell portions along internal and external seams (35, 135).  
15

29. Method according to claim 28 wherein the bonding of said shell portions (41, 42, 141, 142) is carried out using laser welding or ultrasound welding.  
20



**Abstract**

A filter device having filter means, in particular hollow-fibre membranes, arranged in more than one filtration compartment within a filter housing. The filter device thereby  
5 allows more than one filtration process to be carried out serially and/or simultaneously within a single housing. For example a dialysis type filtration process such as haemofiltration or haemodiafiltration or haemodialysis may be carried out at the same time as an ultrafiltration process or as another haemofiltration, haemodiafiltration or haemodialysis process. The device may have a split shell construction bonded or welded  
10 together along longitudinal seams. Internal separating walls within the housing are formed integrally with the shell portions of the housing to form adjacent filtration compartments when the housing portions are joined together.



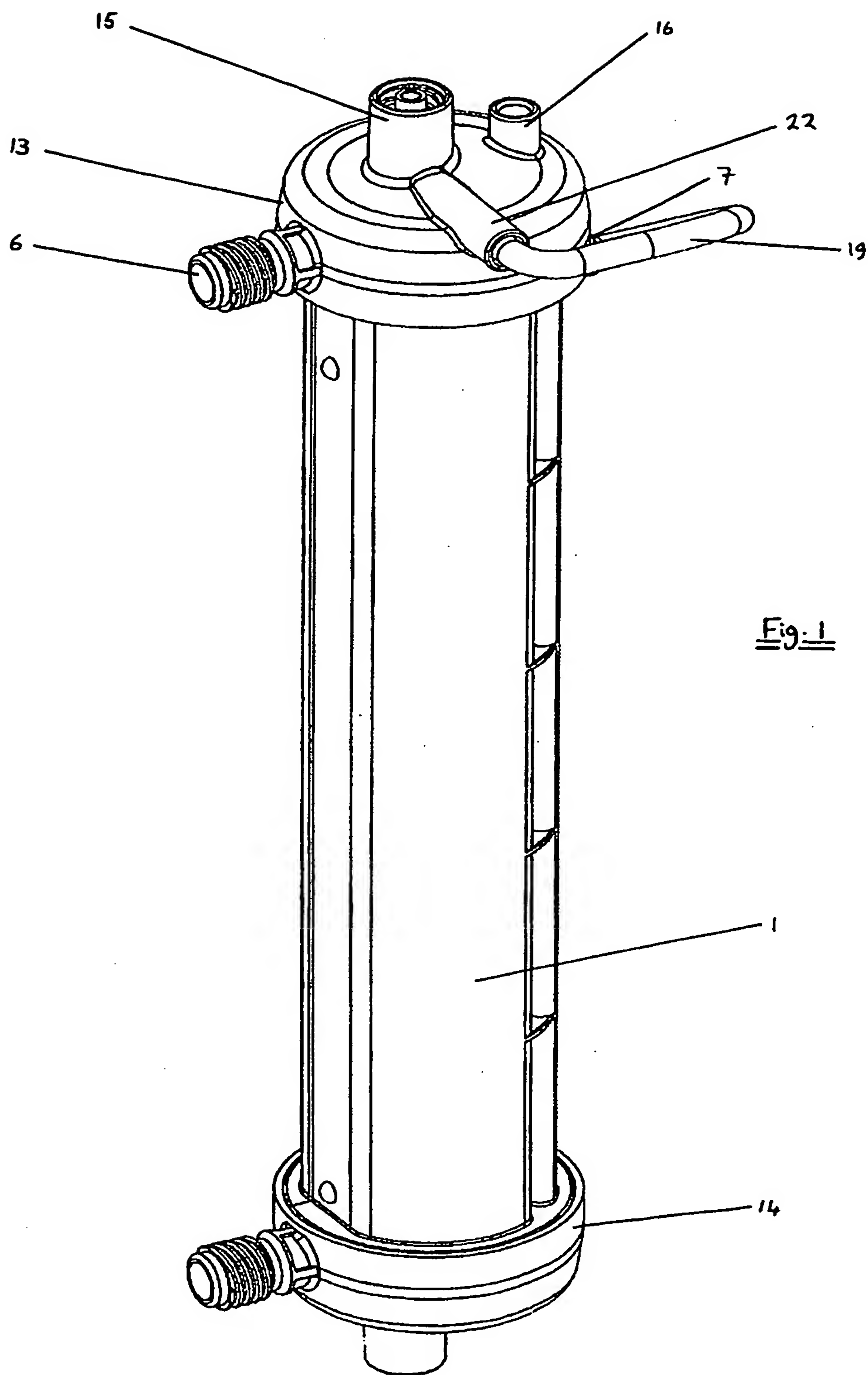


Fig. 1

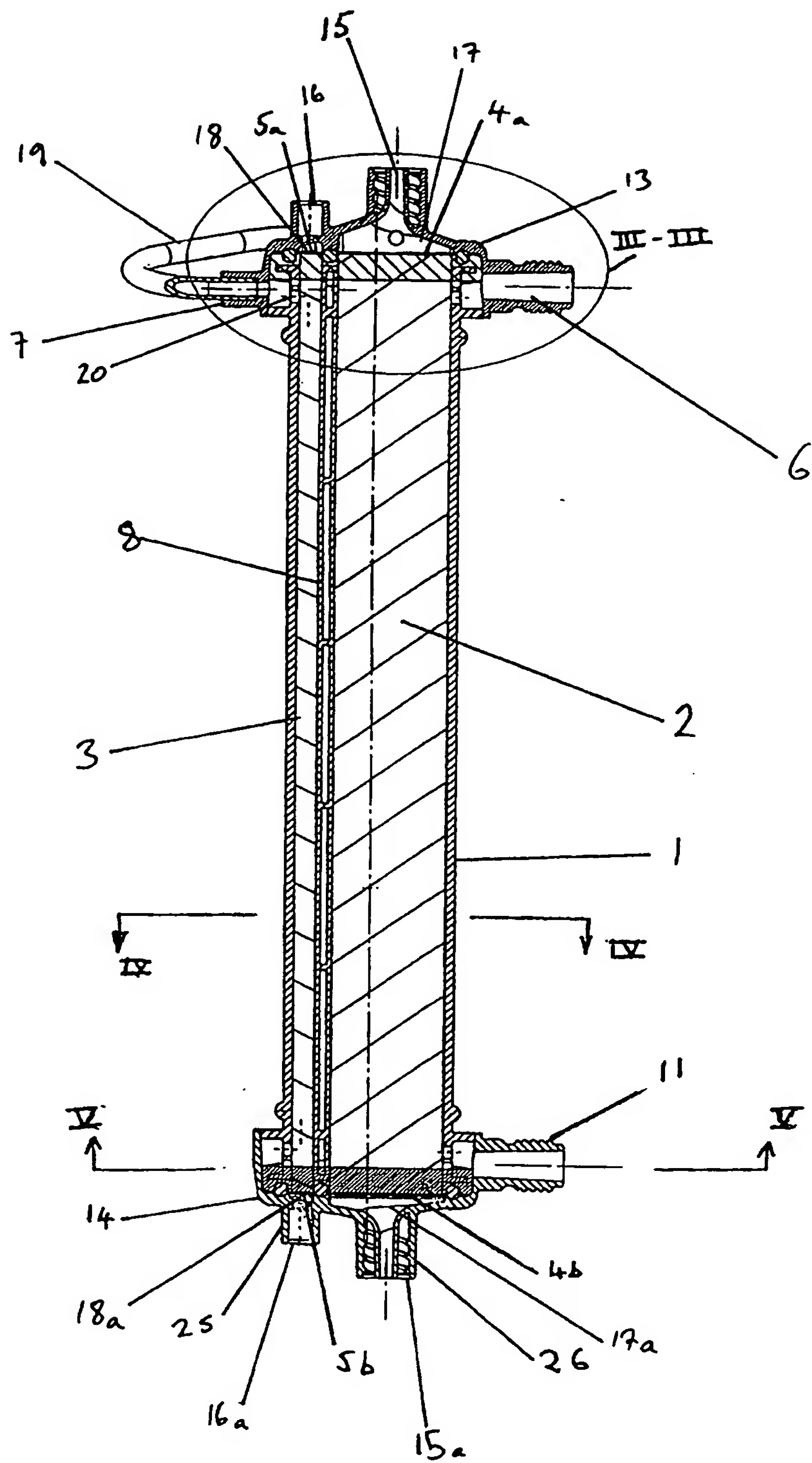


Fig 2

FIG. 3

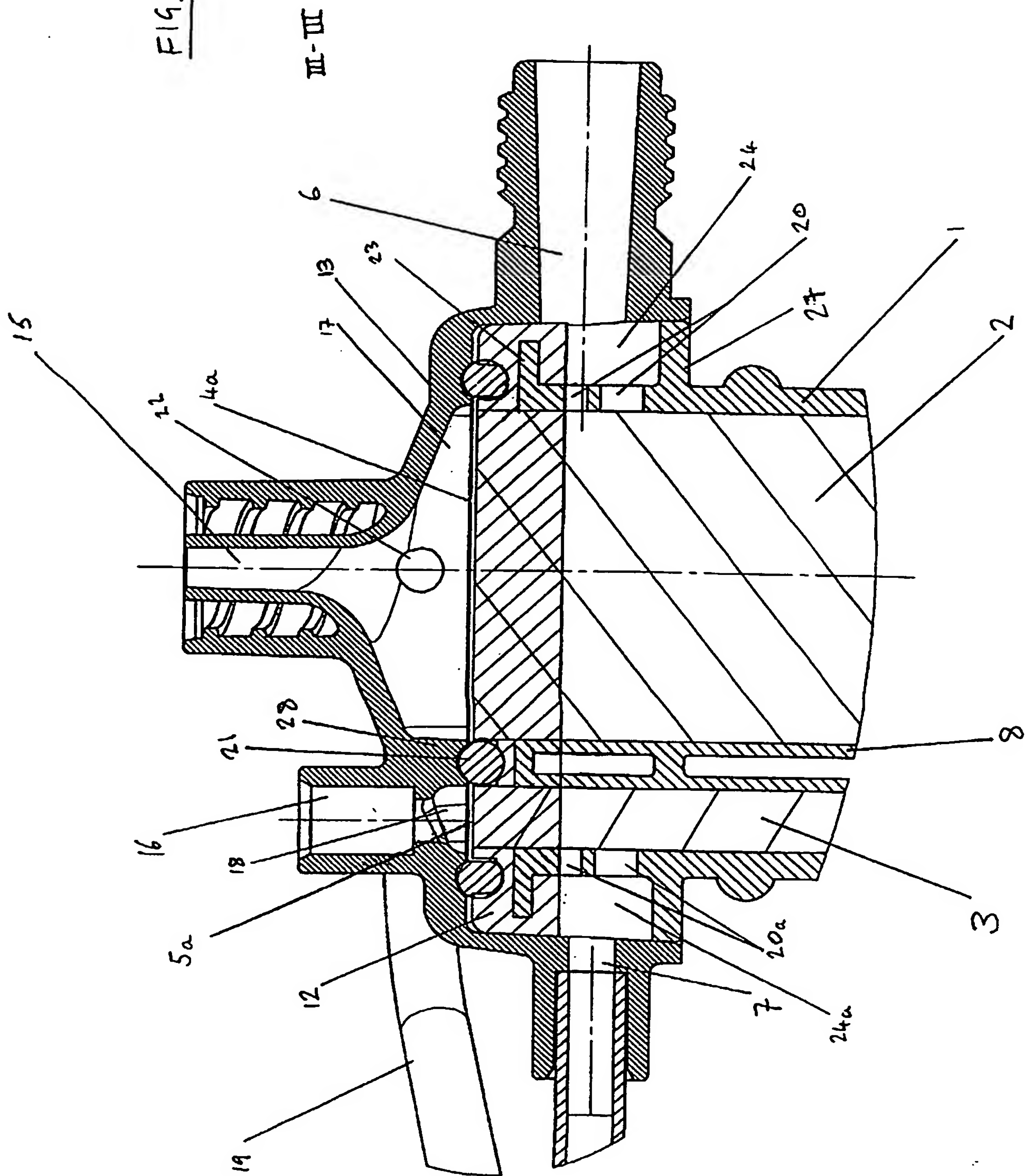


FIG. 4

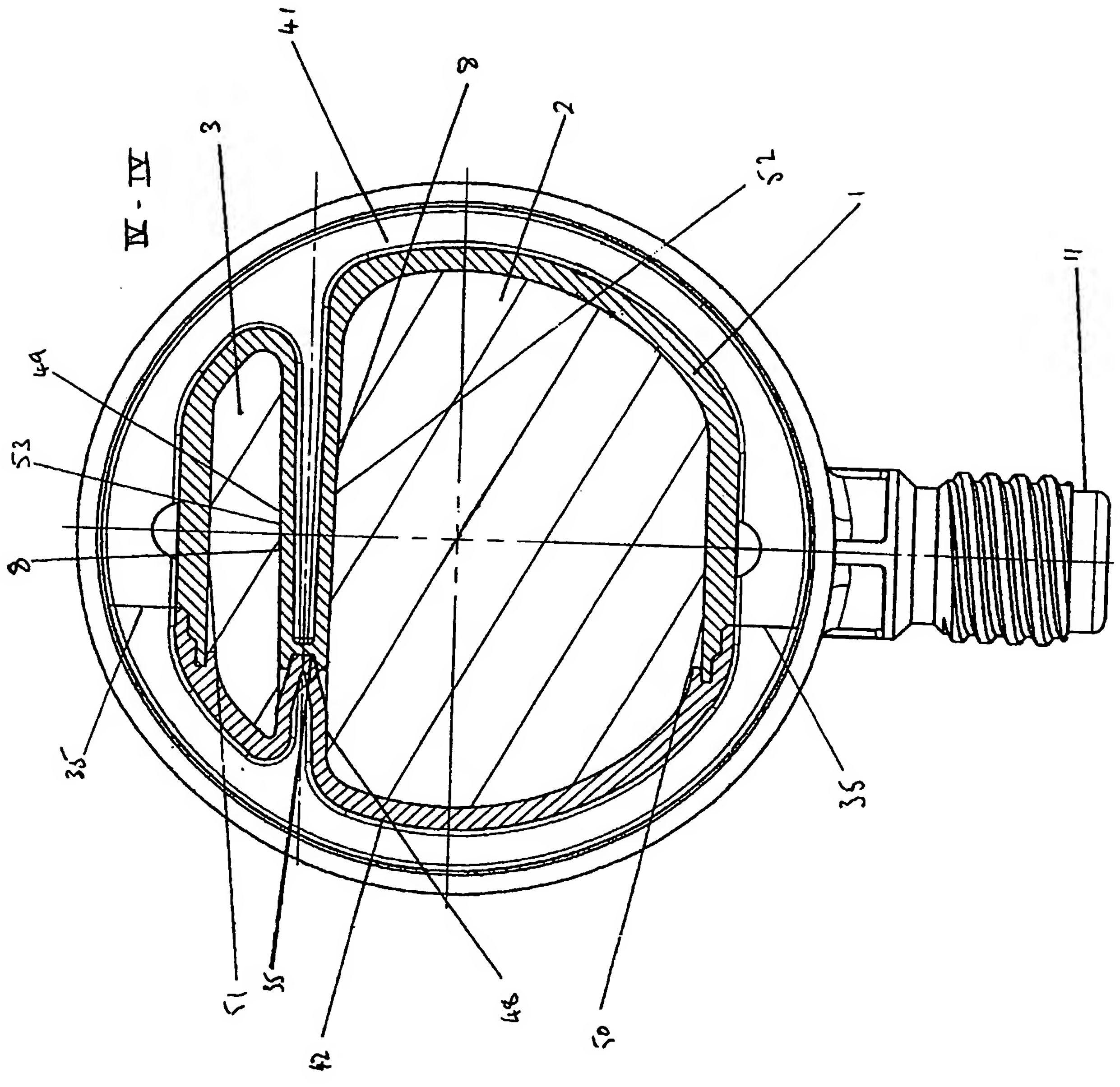
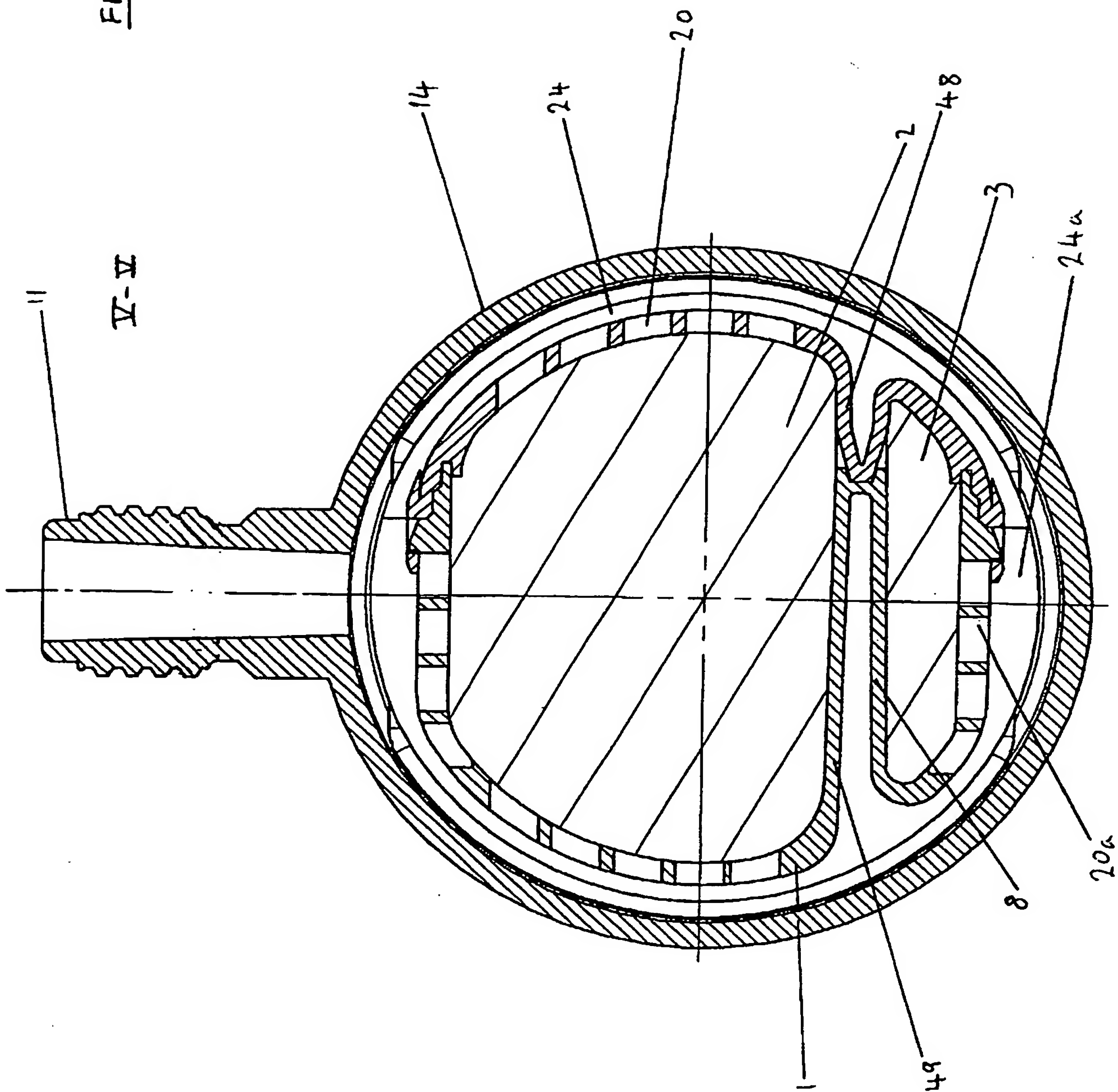


FIG 5



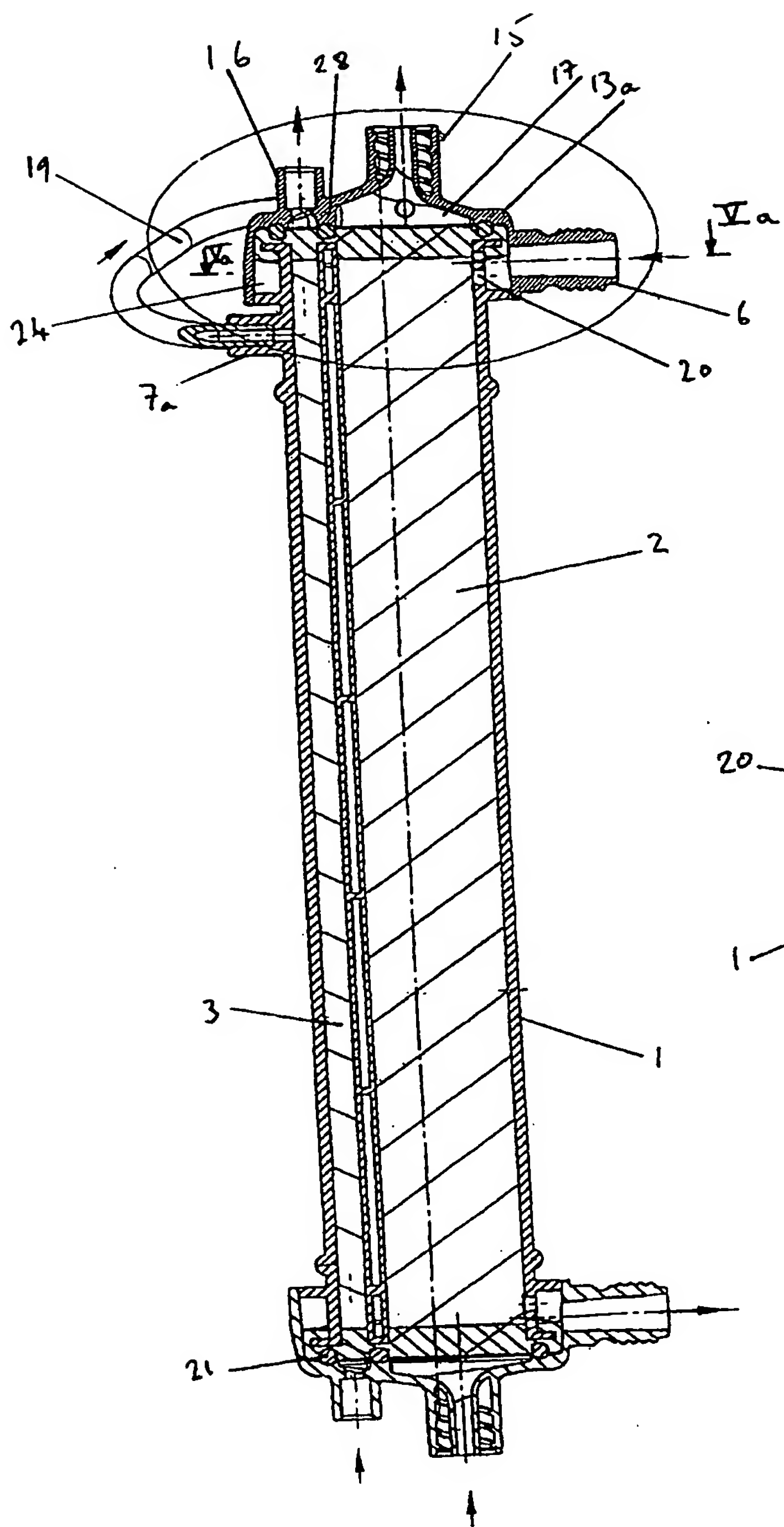


FIG. 2a

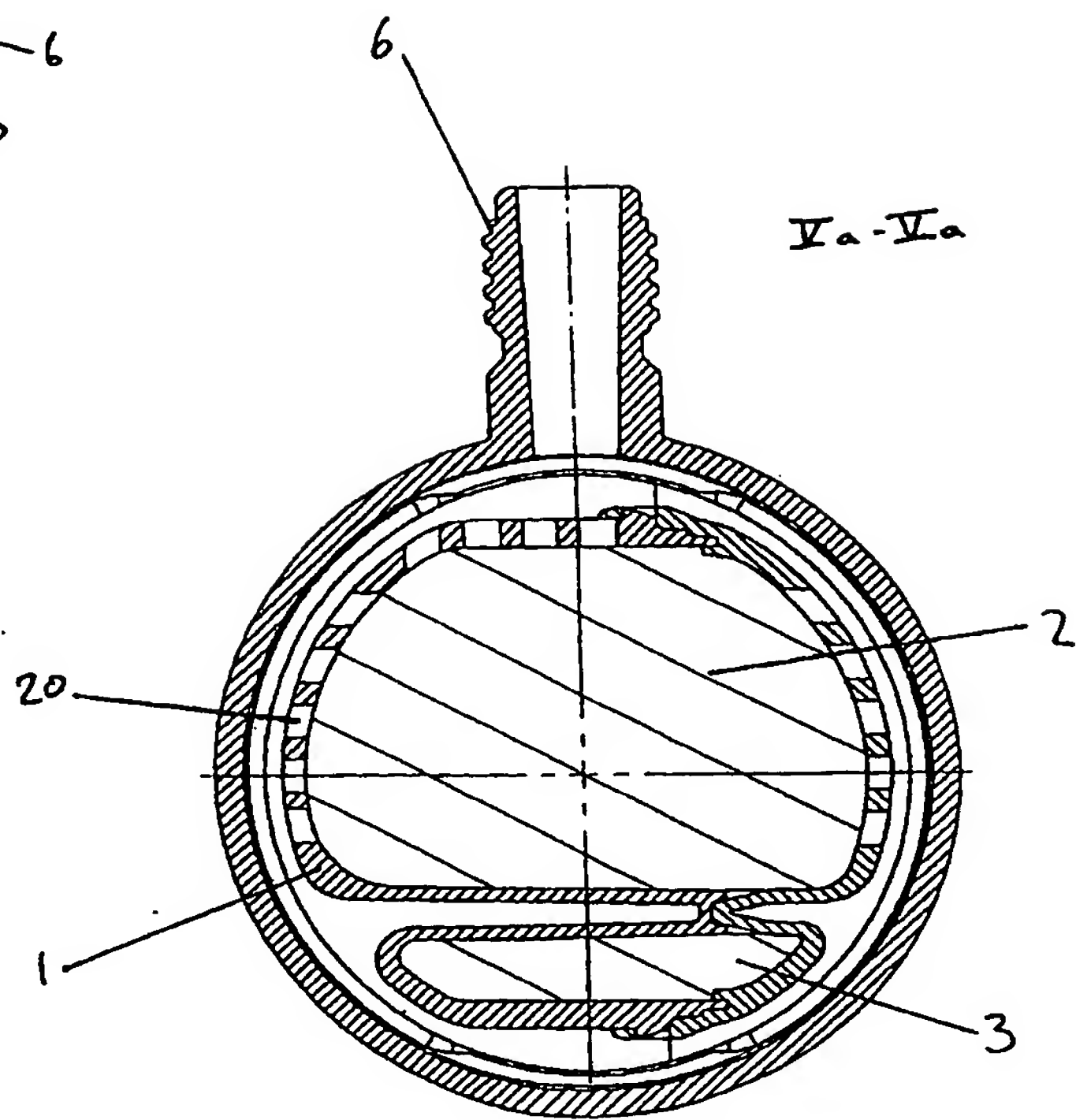


FIG. 5a

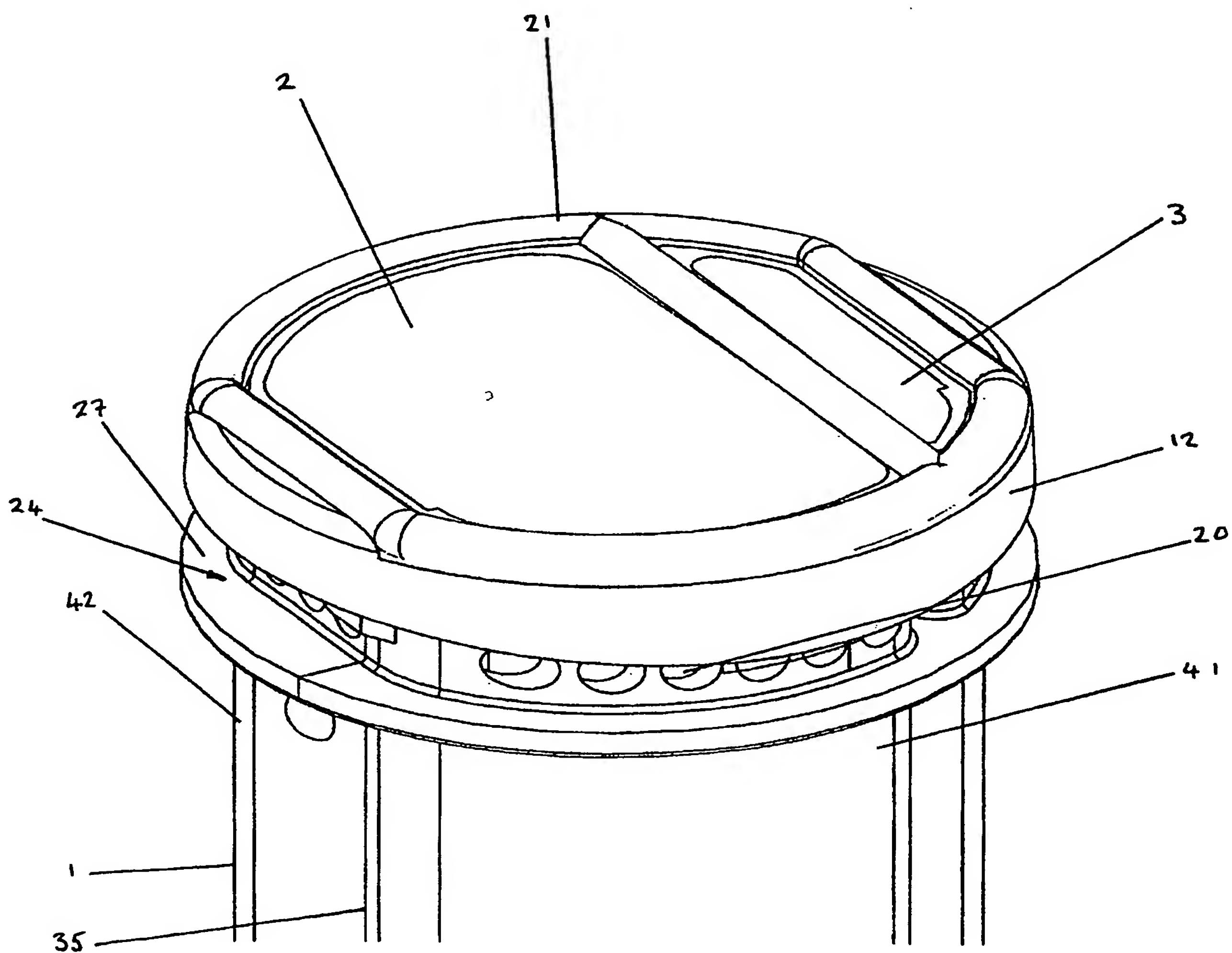


Fig 6

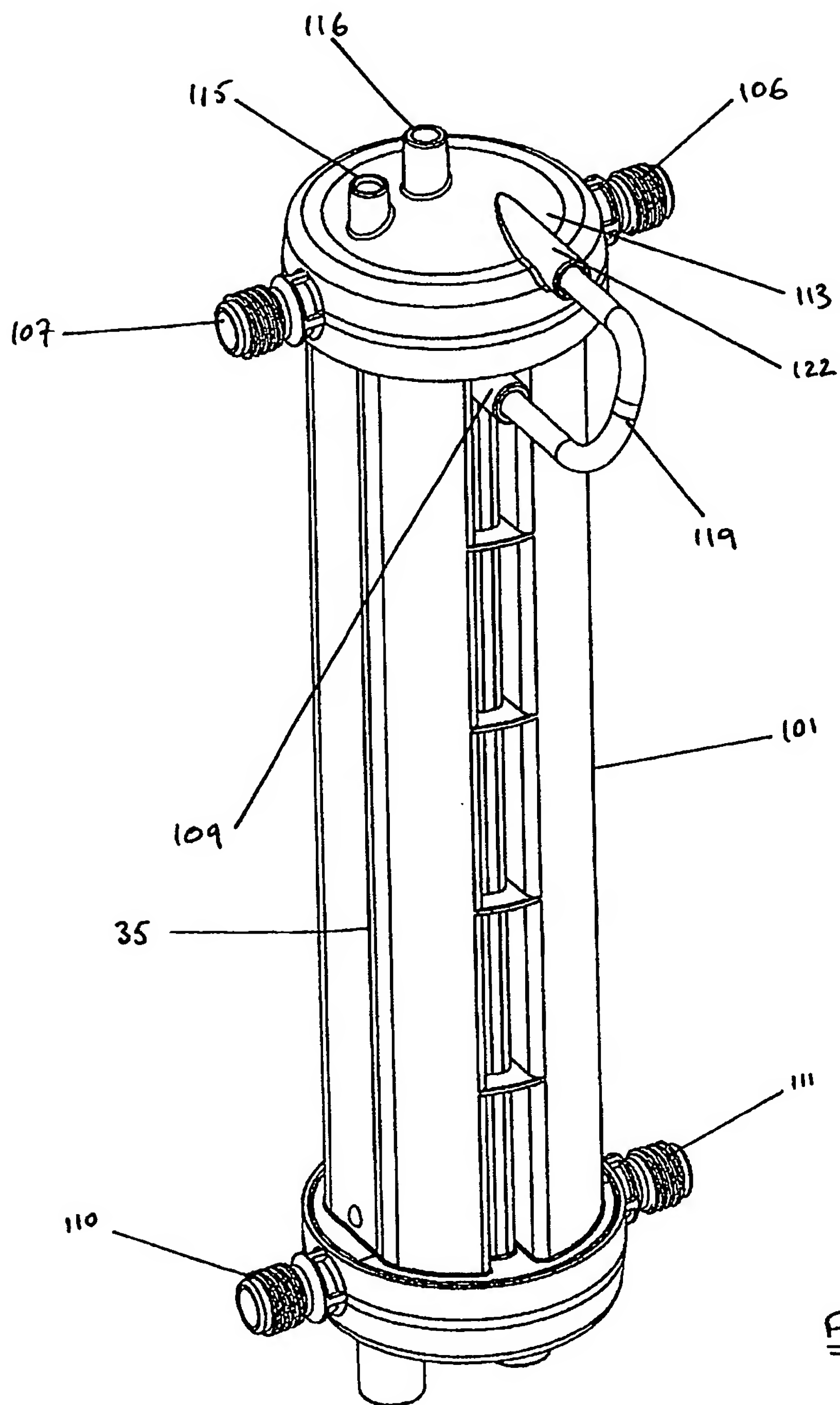


Fig. 7

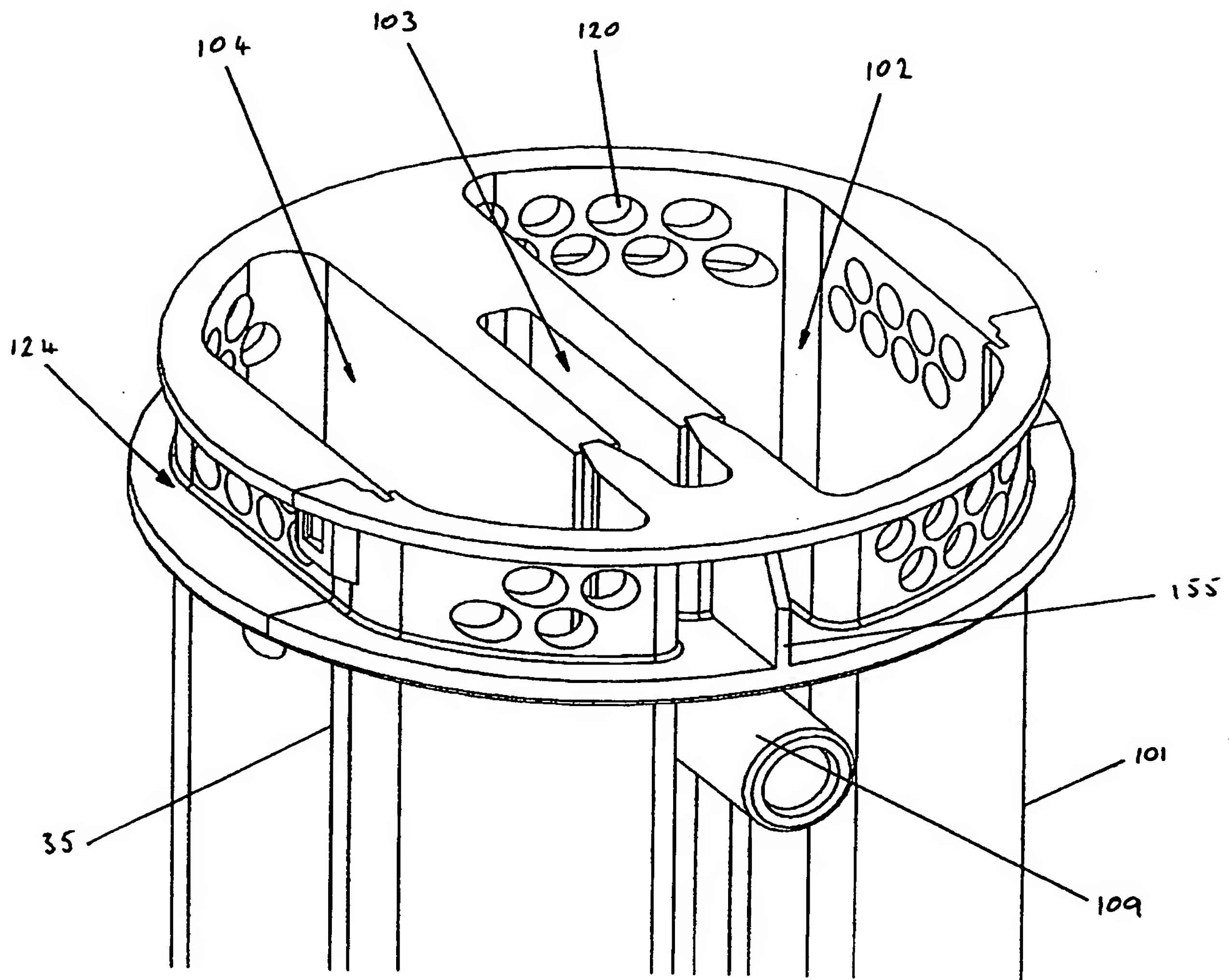


Fig. 8

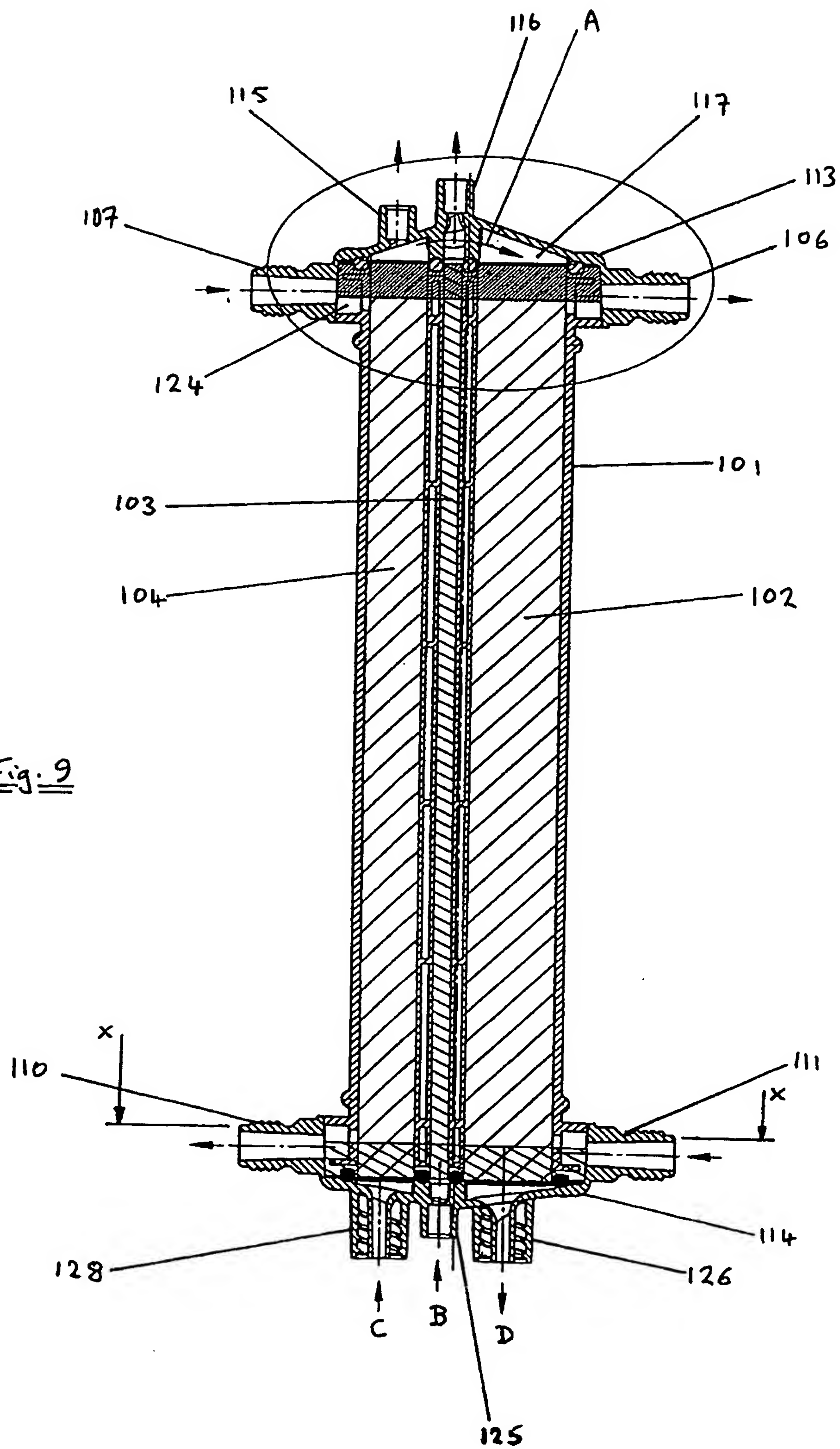


Fig. 9

Fig 11

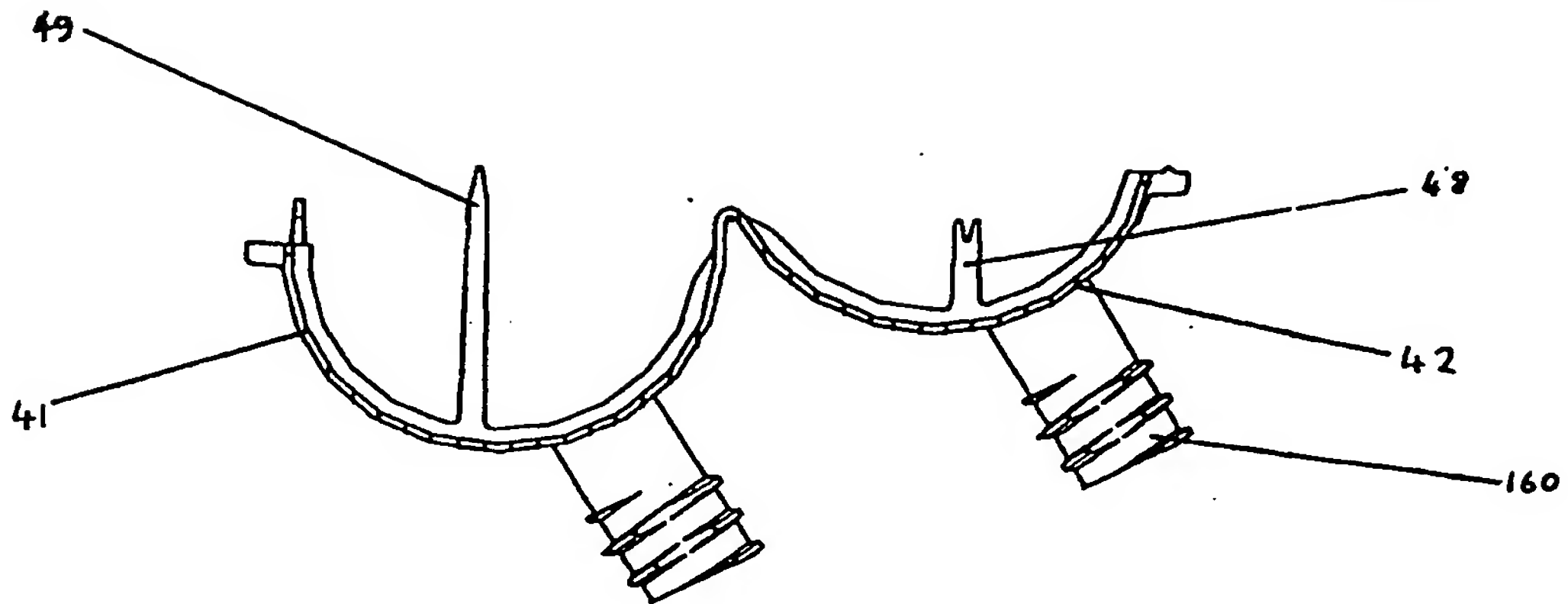


Fig 11a

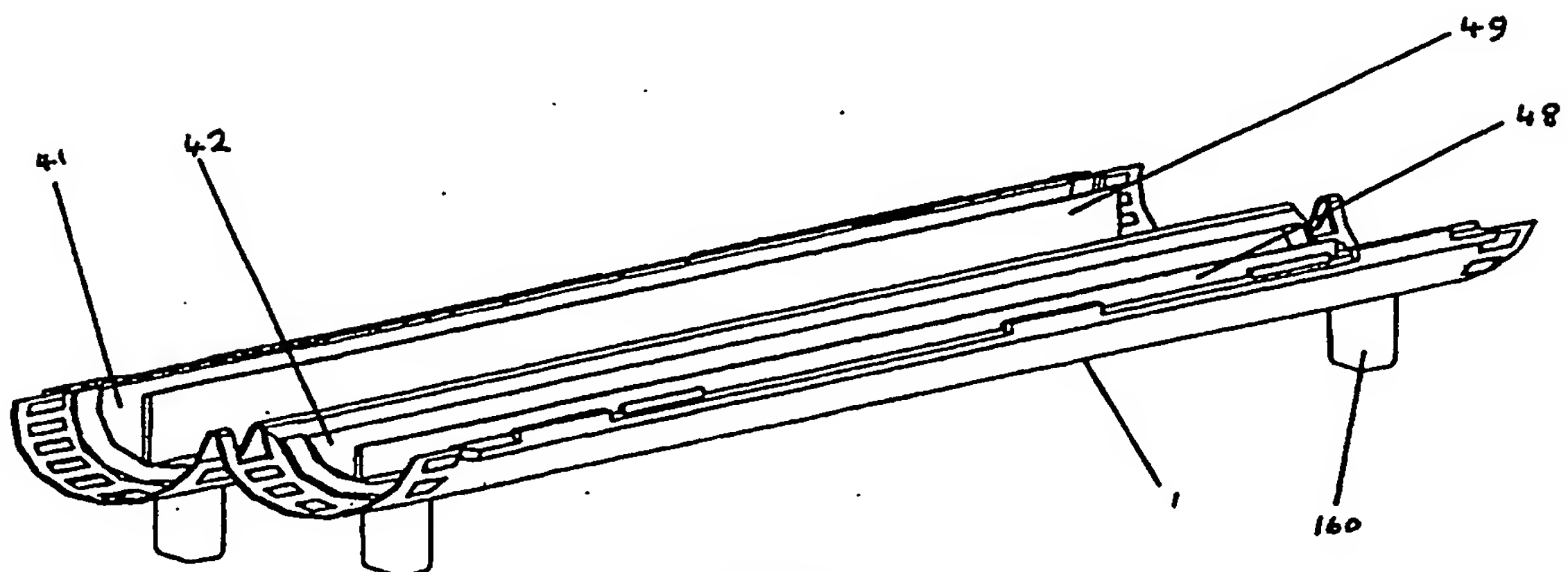
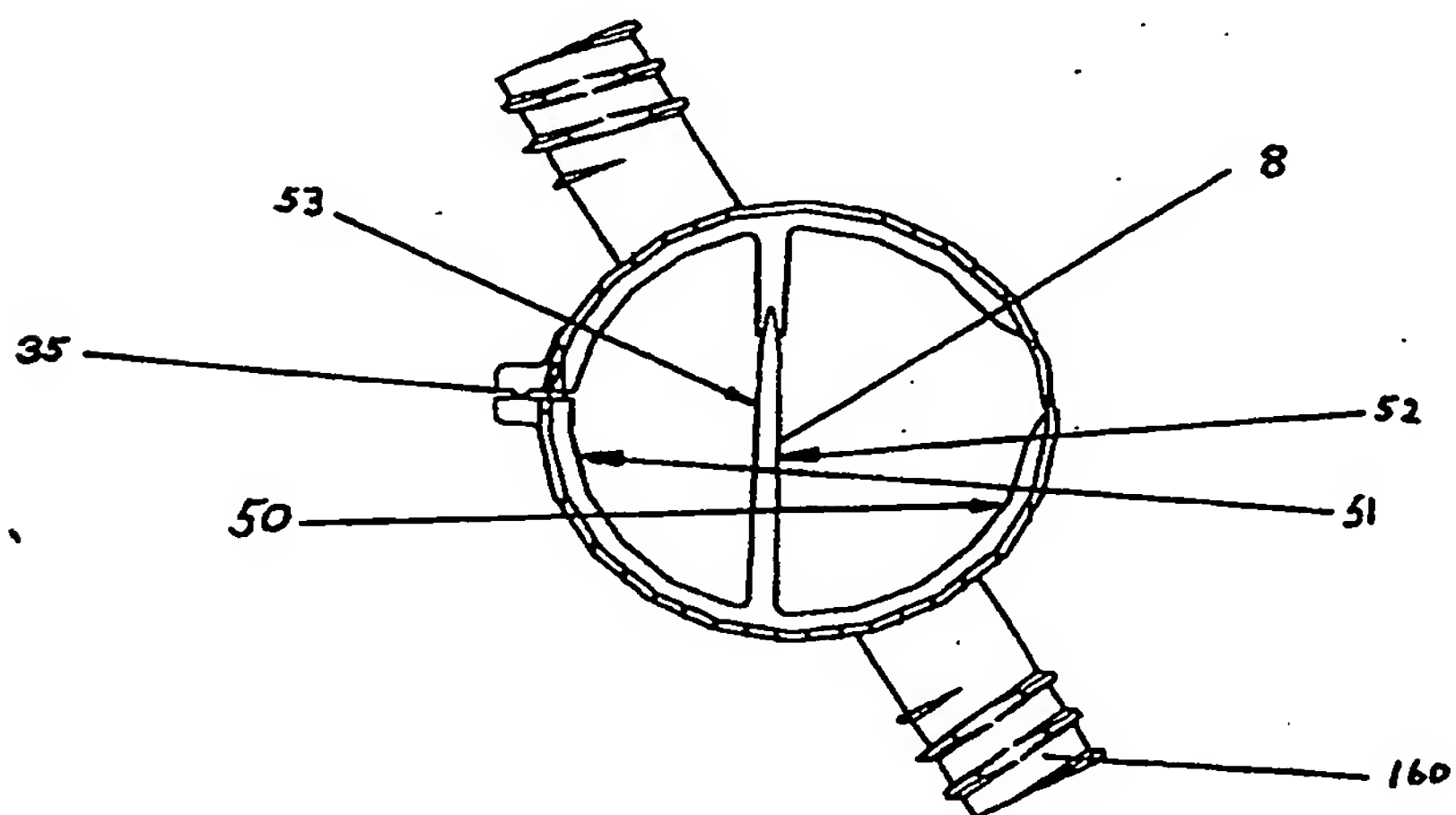


Fig.12

Fig 13

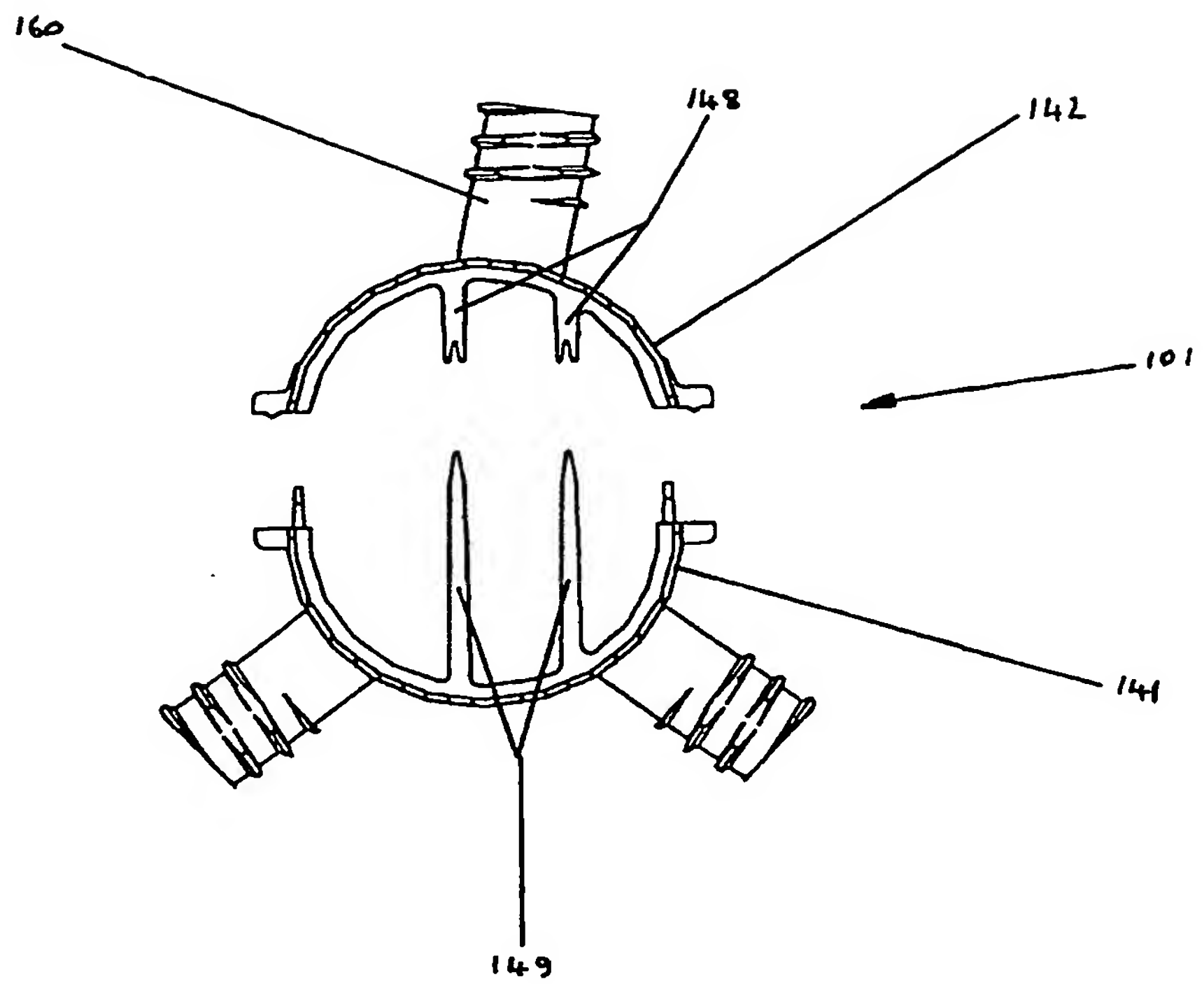
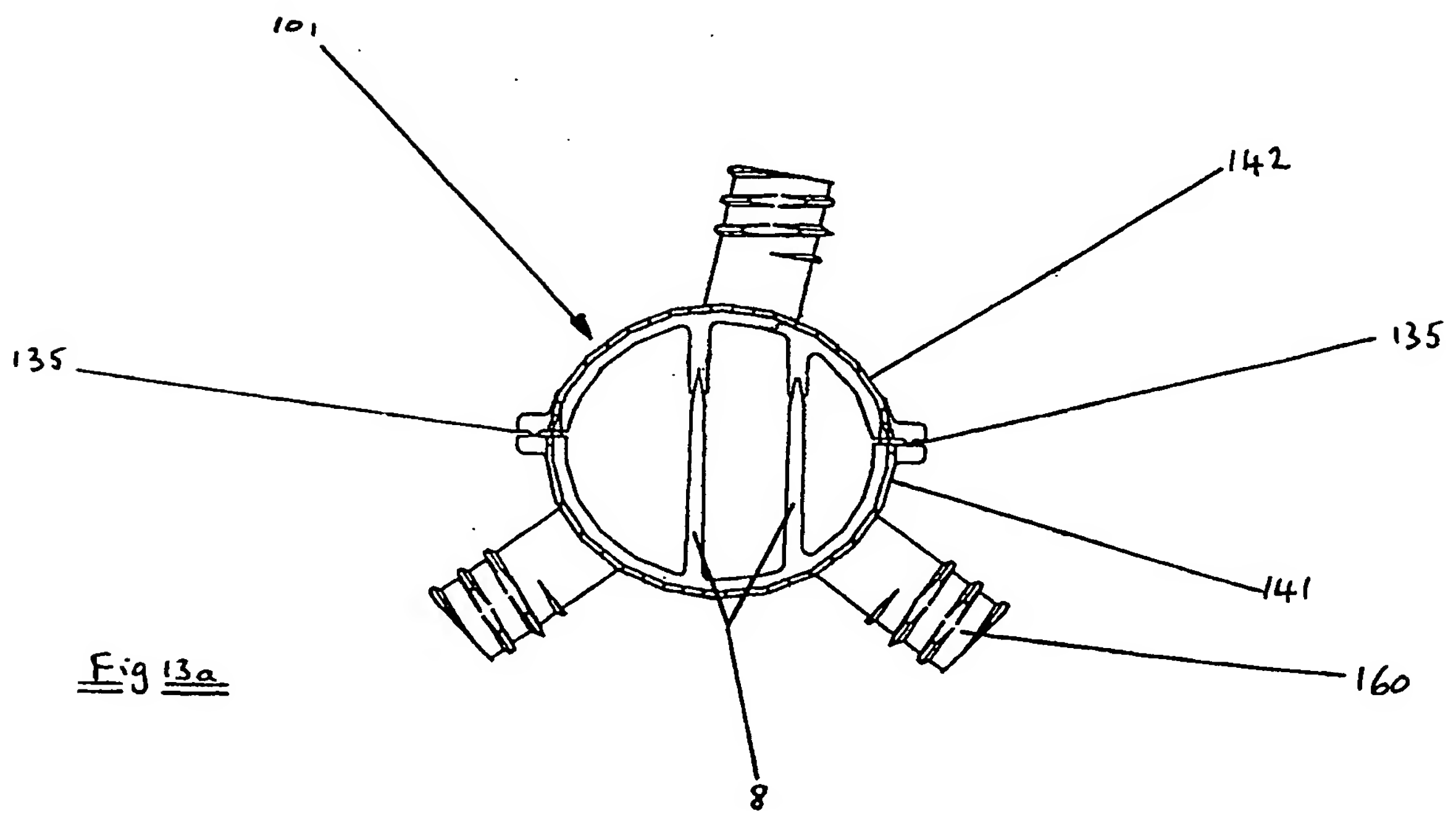


Fig 13a



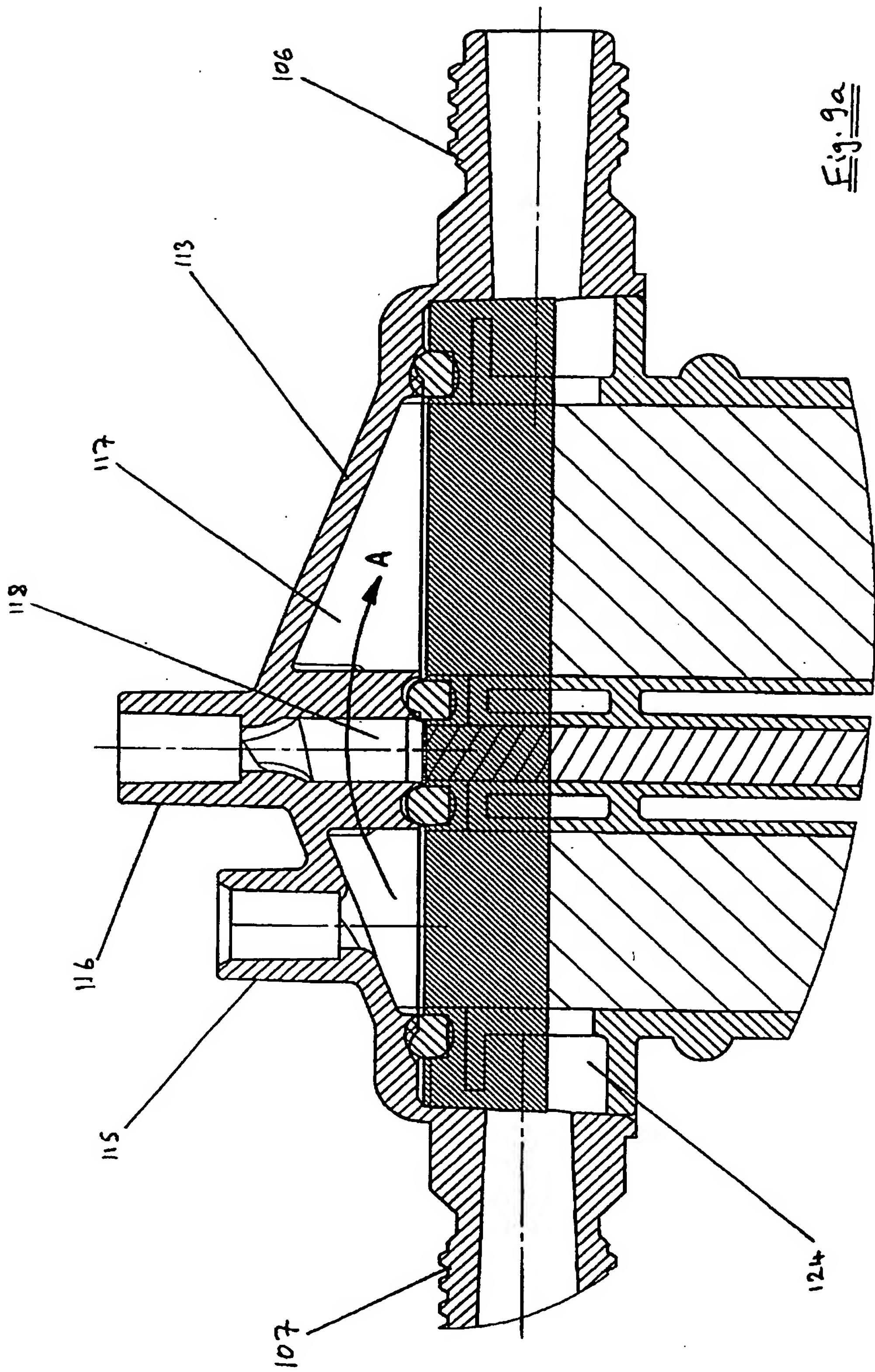


Fig. 9a

